

# Anisotropic ssTEM Image Segmentation Using Dense Correspondence across Sections

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### 1. Membrane segmentation

## 2. Problems

Task: automatic membrane segmentation for anisotropic stacks of ssTEM brain tissue





• Membranes that are not orthogonal to cutting plane are blured (as each image is a projection of the whole thick slice)







Sections from a ssTEM of the Drosophila first instar larva ventral nerve cord (VNC), imaged at a resolution of 4x4x50 nm/pixel (Cardona, A. et al. in PLoS Biol. 10, 2010)



• Neighboring slices are highly different one from another (data is highly anisotropic), so we cannot use methods developed for isotropic data

#### Key idea

- Approximately find corresponding regions in neighboring sections
- Incorporate the context from neighboring sections

### 3. Proposed method





- In order to incorporate the context from neighboring sections, we need to find warping operator F between sections
- We do it by finding Global Dense Correspondence with SIFT Flow (Ce Liu et al. in ECCV 2008)

for a minimum of SIFT flow energy:

• Then concatenate them to

get extended feature vector

• Train Random Forest classifier

with these extended vectors





- Gaussian blur, Sobel filter, Hessian, Gradient,
- Bilateral, Lipschitz, Kuwahara, Gabor, Laplacian, •
- SIFT descriptors, Radon-like features, Ray features,
- Line Filter Transform.

## 4. Graph Cut & Postprocessing

## 5. Results

- We use graph cut segmentation to take into account the fact that the labels of the neighboring pixels are more likely to have the same value.
- Labelling Y is then estimated as argminimum of the following energy:



 $E_{rf}(y_p)$  negative log likelihood of a RF;  $E_s(y_p, y_q)$  smoothness term;

Two examples of the resulted labelling. Original image: (a), (d), no context: (b), (e), our method (c), (f)



 $\lambda_{gf} \sum_{p=1}^{N} E_{gf}(y_p) + \lambda_{gc} \sum_{(p,q) \in \epsilon} E_{gc}(y_p, y_q)$ 

 $E_{gf}(y_p)$  gradient flux term;

 $E_{gc}(y_p, y_q)$  good continuation term.

#### Posprocessing

- Filtering connected regions based on their morphological properties: Area, Solidity, Euler Number and Eccentricity.
- Line Filter Transform:

 $LFT(x_p) = \max_{l \in L_r(x_p)} \int_{z \in l} y_z dz$ 

Where  $L_r(x_p)$  is a set of all the possible lines of the length r.

Results are based on ISBI 2012 challenge results "Segmentation of neuronal structures in EM stacks" (http://bit.ly/riGDUm).

Method	Pixel error	Warping error	Method	Pixel error	Warping error
Human	$6.7 * 10^{-2}$	$3.4 * 10^{-4}$	IDSIA	$6.0 * 10^{-2}$	$4.3 * 10^{-4}$
Dense $ETH$	$7.9 * 10^{-2}$	$6.2*10^{-4}$	CSIRO	$8.7 * 10^{-2}$	$6.8 * 10^{-4}$
Direct $ETH$	$8.0 * 10^{-2}$	$6.5 * 10^{-4}$	Utah	$1.3 * 10^{-1}$	$1.6 * 10^{-2}$
One slice $ETH$	$8.5 * 10^{-2}$	$6.4 * 10^{-4}$	NIST	$1.5 * 10^{-1}$	$1.6 * 10^{-2}$

Our method is **3.6** and **6.4%** more accurate in two different accuracy metrics

than the algorithm with no context from other sections.

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